Source-level spatiotemporal dynamics and interactions (in human intracranial EEG)

Tim Mullen Zeynep Akalin Acar Jason Palmer

2011 Sloan-Swartz Annual Meeting HHMI Janelia Farm Research Campus





To measure and visualize dynamic changes in neural activity and effective connectivity between spatiallylocalized cortical structures that index and predict both neuropathological states as well as healthy cognitive state and behavior



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- Important factors:
 - Accuracy and Validity
 - Spatiotemporal Specificity
 - Scalp and Intracranial EEG



- Post-hoc analyses applied to measured neural activity
- Confirmatory
 - Dynamic Causal Models
 - Structural Equation Models
- Exploratory
 - Granger-Causal methods

Non-Invasive

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Data-drivenSimple, but powerful

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- Scalable (Valdes-Sosa, 2005)

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- Can be (partially) controlled for (unobserved) exogenous causes (Guo, 2008a,b; Ge, 2009)
- Equivalent to Transfer Entropy for Gaussian Variables (Seth, 2009)
- Flexibly allows us to examine timevarying (dynamic) multivariate causal relationships in either the time or frequency domain

- First introduced by Wiener (1958). Later reformulated by Granger (1969) in the context of linear stochastic autoregressive models
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1. Causes should precede their effects in time (Temporal Precedence)

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Granger Causality Axioms

- 1. Causes should precede their effects in time (Temporal Precedence)
- Information in a cause's past should improve the prediction of the effect, above and beyond the information contained in past of the effect (and other measured variables)

Vector Autoregressive (VAR) Modeling



$x_1(t)$	manne manner	$\mathbf{X}(t) = \sum_{k=1}^{p} \mathbf{A}^{(k)}(t) \mathbf{X}(t-k) + \mathbf{E}(t)$
$\begin{array}{c} x_2(l) \\ \vdots \end{array}$	And MAN AND AND AND AND AND AND AND AND AND A	
$x_M(t)$	mmmmm	





























Solution? Source Reconstruction


Solution? Source Reconstruction

 $S(t) = \sum_{k=1}^{p} A^{(k)}(t)S(t-k) + E(t)$



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Solution? Source Reconstruction

 $S(t) = \sum_{k=1}^{r} A^{(k)}(t) S(t-k) + E(t)$

Volume conduction exists for ECoG too!

(c.f. Whitmer, Worrell, ..., Makeig, Frontiers in Neuro, 2010



Solution? Source Reconstruction





Akalin Acar















A Recipe for Reducing Errors:
Anatomically Realistic Forward Model
Appropriately Constrained Inverse Model
Akalin Acar and Makeig, 2010



200 Time (ms)

-31 ms

Group Analysis Visualization

Frequency (Hz)

1:127

Cancel Ok

nDTF [-0.75 0.98828125] [3:7]

{"8", "11", "13", "19", "20",

Cancel

Time (sec)

Make Movie!

Akalin Acar and Makeig, *J. Neurosci. Methods*, 2010 Akalin Acar and Makeig, *IEEE EMBC*, 2008

Subject Folder			
Subject Name	Session Name		
Head Mo	odeling		
nead Modeling			
Resonance Image	Position Data		
Image Segmentation			
Mesh Generation			
	Template Warping		
Source Space Generation			
Electrode Co-Registrati			
FP Solution with BEM	FP Solution with FEM		
Dipole Fitting			



http://sccn.ucsd.edu/nft			
	Subject Folder		
	Subject Name	Session Name	
	Head Modeling		
	From a magnetic Resonance Image	From electrode Position Data	
T1-weighted	Image Segmentation		
	Mesh Generation	Template Warning	
	Source Space Generation	Template traiping	
	Electrode Co-Registrati		
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Akalin Acar and Makeig, *J. Neurosci. Methods*, 2010 Akalin Acar and Makeig, *IEEE EMBC*, 2008







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EEGLAB Software framework



Delorme, Mullen, Kothe, Akalin Acar, Bigdely-Shamlo, Vankov, Makeig, Computational Intelligence and Neuroscience, vol 12, 2011

An Application

Spatiotemporal modeling of seizure causal hubs and propagation dynamics from intracranial EEG



Mullen et al, IEEE EMBC, 2011

Seizure Data





- Pre-Surgical Evaluation
- Rest Data
- 78 ECoG electrodes, 29 Scalp
- Provided by Dr. Greg Worrell, Mayo Clinic

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16 minutes ECoG data, 500 Hz 2 seizures (1.9 min + 1.5 min)























Mullen, Akalin Acar, et al (2011), IEEE EMBC



Mullen, Akalin Acar, et al (2011), IEEE EMBC




ICA Decomposition





channel voltages

Extended Infomax ICA Decomposition X = AS
16 seizure components (ICs) selected



componen activations

Forward Modeling

BEM model

- Plastic sheet (grids)
- Skull (with craniotomy hole)
- Scalp
- Cortex



80 000 source vertices



ICA topographic maps on BEM model





Akalin Acar, et al (2008a,2009) IEEE EMBC

Multi-scale patch-basis source localization with Sparse Bayesian Learning

 $D_{ij} = \text{geodesic_distance}(i, j)$ $D_{ij} = \text{Inf if } D_{ij} > \text{scale}$ $W_{ij}^{(k)} = \text{gauss}(D_{ij}, \sigma_k) = \frac{1}{\sqrt{2\pi\sigma_k^2}} \exp\left(-\frac{D_{ij}^2}{2\sigma_k^2}\right)$ $\sigma_k = \text{scale} / 3$

Three truncated Gaussian patches of different scales

radius	10 mm	6 mm	3 mm		
σ _k	3.33 mm	2 mm	1 mm		
166			66000		
(2)C	MAR.				
	Land?		- Company		
276					
Akalin A	car, et al (200	08a,2009) <i>IEEE EMBC</i>			

nt scales mm	ICA Model	$\begin{aligned} X &= A\hat{S} \\ \hat{S}_q &\coloneqq [1 \times T] \end{aligned}$
	nverse Model	$A_{q} = \tilde{L}\tilde{M}_{q}$ $\tilde{L}^{-1} = SBL(Q)$ $\tilde{M}_{q} = [\tilde{L}^{-1}A]$ $M_{q} = magle a$

Legena					
symb	number of				
т	channels (78)				
V	source voxels (80K)				
С	ICs (16)				
Т	time points (120K)				

 $\begin{array}{l} \text{Poword} \\ X = LS \\ L \coloneqq [m \times v] \text{ Lead Field Matrix} \\ \tilde{L} = [LW^{(1)} \cdots LW^{(3)}]_{m \times 3v} \end{array}$

 $\begin{array}{l} \mbox{POPDOP} & X = A \hat{S} \\ \hat{S}_q \coloneqq [1 \times T] \quad q^{\rm th} \mbox{ IC activation} \\ \end{array} \\ \begin{array}{l} A_q = \tilde{L} \tilde{M}_q + \epsilon_q \\ \tilde{L}^{-1} = {\rm SBL}(A_q, \tilde{L}) \\ \tilde{M}_q = [\tilde{L}^{-1} A_q]_{3\nu \times 1} \\ M_q = reshape(\tilde{M}_q, \nu \times 3) \\ M_q = \sum_{i=1}^3 M_{q(:,i)} \\ P_q = M_q \hat{S}_q \qquad [\nu \times T] \mbox{ cortical surface} \\ potentials \mbox{ for } q^{\rm th} \mbox{ IC} \end{array}$

Ramirez, et al, HBM, 2007

SBL simulation study with MNI model (SNR=50)

Three examples:		Source (x 15)		Max. dis. (mm)	Energy dif.	DF (%)
		Туре	Scale (mm)			
original	reconstructed	Gyral	10	0	1.5	103.8
666		Sulcul	10	1.01	29.8	101.4
		Sulcul	5	2.12	4.1	37.6
		Dual	10	11.6	29.3	89.2
		Gyral	5	1.01	4.7	41.3
		Sulcul	12	1.8	10.6	125.5
		Term		Definition		
		max displacementgeodesic distance between origon reconstructed patch centerenergy difference original energy - reconstructed		original and enters		
				original energy - reconstructed energy		
		degree of focalization (DF) reconstructed energy / or		d energy / origi	nal enegy	
Alcolin Acor at al (INC INC INC INC INC INC INC.		at part part part part part part part pa	1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1 1	

SBL Localization of Epileptogenic IC Sources

IC maps interpolated on cortical surface mesh



Akalin Acar, et al (2009) IEEE EMBC

SBL Localization of Epileptogenic IC Sources

IC maps interpolated on Equivalent Current cortical surface mesh Dipole solution



Radial dipole



Tangential dipole

Akalin Acar, et al (2009) IEEE EMBC



SBL Localization of Epileptogenic IC Sources



Tangential dipole

Akalin Acar, et al (2009) IEEE EMBC

Sulcal source

left



Cortical surface potentials (16 ICs, SBL solution)



playback at 1/5 actual speed

VAR Model Fitting and Multivariate Granger Causality

- Seizure IC activations down-sampled to 256 Hz
- VAR model of order 7 (selected using Hannan-Quinn information criterion) fit to seizure activations using ARFIT algorithm using a 15-sec sliding window with 1 sec step
- Residual whiteness tests (Portmanteau) and stability analysis
- dDTF and spectral density estimated for each window from 1-70Hz
- Significance determined via phase randomization surrogate test



ERSP (spectrum) on diagonal

Time (sec)

Mullen, et al (2011)



ERSP (spectrum) on diagonal

Time (sec)

Mullen, et al (2011)

C: Asymmetric (e.g. causal) connectivity matrix

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Outflow



C: Asymmetric (e.g. causal) connectivity matrix

Outflow

Inflow



C: Asymmetric (e.g. causal) connectivity matrix



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Pre-seizure





Pre-seizure













Pre-seizure Seizure Early Stage Seizure Mid Stage





Pre-seizure Seizure Early Stage Seizure Mid Stage Seizure Late Stage





Spatiotemporal Visualization of Causal Flow Dynamics



Mullen, Akalin Acar, Worrell, Makeig (2011), IEEE EMBC

Causal Flow Dynamics (4-25 Hz)



Mullen, Akalin Acar, Worrell, Makeig (2011), IEEE EMBC



Mullen, Akalin Acar, Worrell, Makeig (2011), IEEE EMBC

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Wes Thompson

Supplementary Slides











Ongoing Work: AMICA

Adaptive Mixture ICA

(Palmer, Kreutz-Delgado, Rao, Makeig, ICASS, 2007)

- Mixture model allowing for robust ICA decomposition of non-stationary processes.
- Affords automated state segmentation based on model likelihoods
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Definitions

 $\begin{array}{ll} X(t) & \mbox{multivariate data at time } t \\ A^h(t) & \mbox{mixing matrix for } h^{\mbox{th ICA model}} \\ S^h(t) & \mbox{source activations for } h^{\mbox{th ICA model}} \end{array}$

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$$p(X(t)) = \sum_{h=1}^{K} p(M_h) p(X(t) \mid M_h)$$
$$p(X(t) \mid M_h) = \left| \det A_h^{-1} \right| p_h(A_h^{-1}X(t))$$
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mixture model

likelihood function

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likelihood function

generative model

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Seizure segmentation using AMICA model likelihoods

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AMICA - SBL Solutions

Representative component maps and SBL solutions from the Amica model which is dominant in late seizure stage



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Akalin Acar, Palmer, et al (2011), IEEE EMBC





Akalin Acar, Palmer, et al (2011), IEEE EMBC



2nd cluster



Akalin Acar, Palmer, et al (2011), IEEE EMBC





2011)

Akalin Acar, Palmer, et al (2011), IEEE EMBC





AMICA Dependency Clusters

Seizure clusters

Pre-seizure clusters





4th cluster

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AMICA Dependency Clusters



Akalin Acar, Palmer, et al (2011), IEEE EMBC

Mullen, et al (2011) IEEE EMBC

AMICA Source Activations



3 seconds data from AMICA model which dominates in second seizure period